

METHOD FOR PRODUCING A CONTROLLED-RELEASE PREPARATION

## FIELD OF THE INVENTION

The present invention concerns a method for producing a pharmaceutical preparation. Specifically the invention concerns a method for producing a controlled-release pharmaceutical preparation with a particle-containing coating. The invention also concerns new pharmaceutical preparations.

## BACKGROUND OF THE INVENTION

Many polymers are used as coatings in controlled release oral pharmaceutical preparations. These polymers are essentially water-insoluble and have consequently low permeability towards water and drugs. If the drug is very soluble and surface of the preparation is large, as in e.g. pellets, low permeability is desired. If the drug is moderately soluble or the surface of the preparation is small, as in e.g. tablets, the permeability of the coating has to be increased.

One method of increasing the permeability of the polymer is disclosed in the US patent 4 629 619. According to this patent the permeability is increased by including water soluble particles in the coating. When the preparation is subsequently swallowed by a patient and contacted with the GI juices, the water soluble particles dissolve and form pores or channels in the coating through which pores or channels the drug is released from the preparation. The coating including these water soluble pore-forming particles is obtained by a method according to which the water-soluble particles are suspended in an organic solvent. Medical preparations developed according to this patent are currently used and well accepted by the patients. A disadvantage is however the necessity to use organic solvents.

Another method of increasing the permeability is disclosed in the US patent 5 472 712 and 5 639 476. Ac-

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cording to these two patents the permeability of the polymer is increased by including a water-soluble material in the polymer. The coating including the water soluble material is obtained by dissolving the water soluble material in the aqueous dispersion of a film-forming polymer. When such a preparation is subsequently swallowed and contacted with the GI juices the water soluble material dissolves and make the polymer coating micro-porous and increase the release rate of the drug through the coating. The sizes of the micro-pores correspond to those of the dissolved molecules. An advantage with medical preparations prepared according to these two patents is that they may be prepared without organic solvent. A disadvantage is that the mechanical strength of the coating is poor, when the permeability is increased to an acceptable level for moderately soluble drugs, especially for tablets. Another disadvantage is that the size of the pores is not controlled which means e.g. that it is difficult to obtain reproducible products.

The permeability increasing or pore-forming agents used according to the two above methods may be identical chemically but the physical state of these agents in the coating solution is different.

#### OBJECT OF THE INVENTION

An object of the present invention is therefore to accomplish a method for producing a controlled-release pharmaceutical preparation having the same effective release rate and mechanical strength as the one described in US 4,557,925 while avoiding the use of organic solvents and the problems arising by using the method according to US 5,472,712 and 5 639 476.

#### SUMMARY OF THE INVENTION

This object as well as other objects that will be apparent from the description below, have now been obtained according to the present invention by providing a method for producing an essentially zero order, con-

trolled-release pharmaceutical preparation with a particle containing coating according to claim 1.

This method comprises the steps of:

- preparing a drug-containing solid core;
- 5 suspending a pore-forming agent having a balanced solubility in an aqueous dispersion of a film-forming, water insoluble polymer in order to form a coating suspension having a predetermined amount of solid particles of the pore-forming agent suspended therein;
- 10 coating the solid core with the obtained suspension; and drying the coated tablet.

By a careful selection of the type, amount and particle size of the pore-forming agent, the coating of the final tablet will contain comparatively large particles

15 of the pore-formers. When the tablet is then contacted with the GI juices of a patient, these particles dissolve and create a network of canals or pores of a predetermined size in the polymer coating and the drug is released through these pores or canals. Due to this network

20 the coating will get good mechanical stability and the polymer film will be left intact after the release of the drug.

A predetermined release rate may be obtained by selecting the above parameters of the pore-forming agent in

25 combination with type and amount of film forming polymer. The coatings thus prepared have a good mechanical stability and are left intact after the release of the drug and the pore-forming agent.

The problem to be solved by the present invention is

30 thus to find a pore-creating agent or pore-former combining the two seemingly non compatible properties of being, on one hand sufficiently insoluble in the aqueous coating dispersion, and on the other hand sufficiently soluble in the aqueous GI juices. In this context this feature is

35 referred to as "balanced solubility".

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## DETAILED DESCRIPTION OF THE INVENTION

The critical pore-forming agent must be a pharmaceutically acceptable substance that can be added to the aqueous dispersion of the film-forming polymer without being completely dissolved. Important factors for the pore-forming agent are its solubility and mean particle size. The solubility of the pore-forming agent is below 200 mg/ml in the coating solution at 25°C. Preferably the solubility is below 100 mg/ml, more preferably below 50 and most preferably below 30 mg/ml.

The mean particle size of the pore-forming agent when added to the coating solution is 0.1-500  $\mu\text{m}$ , preferably 0.5-100  $\mu\text{m}$  and most preferably 1.0-25  $\mu\text{m}$ .

If larger particles are used it will be difficult to get reproducible preparations and if smaller particles are used manufacturing problems are expected.

The predetermined amount of solid particles of the pore-forming agent in the coating solution is selected by the man skilled in the art in view of the specific drug and polymer used and the desired release rate.

In a preferred embodiment of the invention the pore-forming agent is selected from the group consisting of potassium hydrogen tartrate (potassium bitartrate), creatine, aspartic acid, glutamic acid and inosine.

Other preferred pore-forming agents are chitosan and poly(butyl methacrylate, (2-dimethyl aminoethyl) methacrylate, methyl methacrylate) 1:2:1.

Other pore-forming agents which may be used selected from a group consisting of potassium salts, calcium salts, magnesium salts, amino acids, weak acids, carbohydrates, polymers with amino and/or acid functions. Examples are asparagine, glutamine, leucin, neroleucine, isoleucine, magnesium citrate, magnesium phosphate, magnesium carbonate, magnesium hydroxide, magnesium oxide or a composition wherein at least one component is selected from one of these substances.

The film-forming polymer according to the present invention could be any pharmaceutically acceptable water insoluble or essentially insoluble polymer, block- or co-polymer that can be dispersed in an aqueous solution. Example of such polymers are polymers selected from the groups consisting of cellulose esters, acrylic polymers, polyvinyl acetates, polyvinyl chlorides or a composition wherein at least one component is selected from one of the groups.

Other preferred coating polymers are ethylcellulose, celluloseacetate, celluloseacetatebutyrate, celluloseacetatepropionate, nitrocellulose, polymethyl-methacrylate, poly(ethylacrylate, methylmetacrylate), polyvinylacetate, polyvinylchloride, polyethylene, polyisobutylene, poly(ethylacrylate, methylmetacrylate, trimethylammonioethylmetacrylatechloride).

30 In another preferred embodiment of the invention the coating polymer is a copolymer consisting of 50-100% by weight of polyvinylchloride and 0-50% by weight of polyvinylacetate.

The weight ratio, amount of pore-forming agent to  
35 total weight of the dry coating, depends on the chosen  
polymer and pore-former and the release pattern desired.

but is normally between 40 and 95, preferably between 50 and 90 and most preferably between 55 and 88% by weight.

A plasticiser may be added to adjust the softening temperature (T<sub>g</sub>) of the polymer. The T<sub>g</sub> is an important factor for regulating the mechanical properties of the polymer. Examples of suitable plasticisers are acetyltributyl citrate, acetyltriethyl citrate, castor oil, diacetylated monoglycerides, dibutyl sebacate, diethyl phthalate, glycerin, mono- and diacetylated monoglycerides, polyethylene glycol, propylene glycol, triacetin, triethyl citrate.

The pore-forming agent in the coating suspension is preferably stabilized with one or more ionic, non-ionic or polymer surfactants. Examples of suitable surfactants are diethanolamine, fatty acids, HPMC (hydroxy propyl methyl cellulose), HPC (hydroxy propyl cellulose), monoethanolamine, nonoxynol, octoxynol, oleic acid, poloxamer, polyoxyethylene 50 stearate, polyoxyl fatty acid, polyoxyl hydrocarbon ether, polysorbate, povidone, salts of fatty acids, sodium lauryl sulfate, sorbitan ester, trolamine.

The aqueous dispersion of the polymer and the pore-forming agent may be used to coat solid cores, which in this context includes crystals, granules, pellets, tablets or the like.

The aqueous dispersion of the polymer and the pore-forming agent is preferably spray-coated onto the solid cores.

The obtained, coated cores may be cured with heat or moisture. Thus the coated preparation may be cured at a temperature higher than storage condition and at a humidity that could be specified for a period of time until the curing endpoint is reached. This endpoint is determined by comparing the dissolution profile with the profile from an accelerated storage condition, for example 3 months at 40°C at ambient humidity. The curing may take

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place in the coating equipment or in a separate dryer as for example in a drying chamber or a drying vessel.

The drug in the solid core could for example be tranquillizers, antibiotics, hypnotics, antihypertensives, antidiabetics, diuretics, antikolinergics, antihyperacidics, antiepileptics, ACE inhibitors,  $\beta$ -receptor antagonists and agonists, anaesthetics, anorexiant, antiarrhythmics, antidepressants, anticoagulants, antidiarrhoetics, antihistamines, antimalarials, antineoplastics, immunosuppressives, antiparkinsonians, antipsychotics, antiplatelets, diuretics or antihyperlipidics.

The drug substance could for example be potassium chloride, theophylline, a theophylline salt, phenylpropanolamine, sodium salicylate, paracetamol, carbidopa, levodopa, diltiazem, enalapril, verapamil, naproxen, pseudoephedrin, nicorandil, oxybutuin, morphine, oxycodone or propranolol.

The aqueous suspension of pore-former and polymer can be diluted with an organic solvent up to 20%, preferably up to 10% and most preferably up to 5%. The organic solvent plasticises the polymer to enhance film formation. The organic solvent also decreases the solubility of the pore-former in the suspension. Thus by using a small amount of organic solvent some advantages may be obtained and, compared with the presently used system, the amount of organic solvent can be reduced. According to the preferred embodiment no organic solvent is included.

In its method aspect, the present invention is not limited by the drug or type of drug incorporated in the preparation. Any composition containing any presently known or future discovered orally acting drug may be coated in order to provide the highly advantageous controlled release pharmaceutical preparations of the present invention.

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5       The invention is further illustrated by, but should not be limited to, the following preparations and example.

10. Core

TABLE 1

Ingredients	(mg/tablet)
Diltiazem hydrochloride	350
Sodium dihydrogen citrate	218
Povidone K25	42,4
Magnesium stearate	12,5
Ethanol*	45,4
Total	623

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The composition of a coating is shown in table 2. The coating suspension was prepared by adding the polymer dispersion, the pore former (with a specific particle size of 25 $\mu$ m) and deionised water to a final content of dry substances of 15% w/w, to a container with continuous stirring.



TABLE 2

Ingredients	(%/coating)	Dry weight (mg)
Polymer dispersion- Polyvinylacetate (wa- ter dispersion)	30	21
Potassium bitartrate (KHT)	70	49
Deionised water*		397*
Total (mg)		70
Total (mg/cm <sup>2</sup> )		20

\*Evaporates during the process

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#### Coating

The cores were coated with the coating suspension in a coating pan. The coated tablets were allowed to dry in the pan for 15 minutes.

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Different embodiments of the preparation according to the invention, shown in table 3, were made accordingly.

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TABLE 3

Batch	Core (Diltiazem)  (mg)	Coating				
		Film weight  (mg/cm <sup>2</sup> )	Pore- former  Type (%)		Polymer  Type (%)	
1	350	20	KHT <sup>1</sup>	0	PVAc <sup>2</sup>	100
2	350	4, 8	KHT <sup>1</sup>	0	PVAc <sup>2</sup>	100
3	350	20	KHT <sup>1</sup>	80	PVAc <sup>2</sup>	20
4	350	20	KHT <sup>1</sup>	60	PVAc <sup>2</sup>	40
5	320 <sup>3</sup>	24	KHT <sup>1</sup>	70	P(EA-MMA) <sup>4</sup>	30

<sup>1</sup> KHT=Potassium bitartrate

<sup>2</sup> PVAc=Polyvinylacetate

5 <sup>3</sup> 100 mg of Polyethyleneoxid is included in the formulation

<sup>4</sup> P(EA-MMA)=Poly(ethylacrylate-methylmethacrylate) 2:1

### Results

10 Table 4 shows results from an in vitro dissolution test (according to USP 23, paddle method) with the formulations from table 3.

15 Batch number 1 and 2 with no added pore-former have a very slow release pattern. The addition of pore-former (batch 3-5) increases the release rate and makes it possible to design formulations according to a desired release pattern.

20 Batch 2 and 4 had comparable drug-release rates. However, the polymer films from batch 2 ruptured during the analysis. Batch 4 showed much less variability in drug release compared to batch 2 and the polymer film still had good mechanical strength after the analysis.

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TABLE 4

Batch	Amount released Diltiazem (%) after x hours (pH 6,8)							Range at 40% re- leased Diltiazem	
	2h	4h	8h	12h	24h	48h	96h	(%)	n
1	0,1	0,1	0,1	0,1	0,1	0,1	0,6	-	6
2	3,7	7,0	14,9	22,2	41,7	89,4	101,3	17,7	3
3	26,8	50,8	81,6	93,2	97,0	-	-	2,2	6
4	0,6	1,5	8,5	19,7	41,2	-	-	3,5	6
5	15,0	35,1	65,1	89,3	101,4	-	-	7,2	6

After the 24 h in vitro dissolution test the tablet  
5 residuals (= the polymer films filled with water) were  
tested for mechanical strength (MS). The force required  
to crack the polymer film was recorded.

The following results were obtained.

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TABLE 5

Batch	1	2	3	4	5
MS (N)	-	0	20	27	18

The same test performed on preparations according to  
the US patent 5 472 612 demonstrated that the polymer  
films were broken with negligible forces i.e. forces well  
below 1 N.

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The following tables show the effect of the particle size on the release rate.

TABLE 6

Batch	Core Diltiazem	Coating	Pore-former			Coating Polymer P (EA-MMA)
	(mg)	Film Weight (mg/cm <sup>2</sup> )	Type	Particle size ( $\mu$ m)	Amount (%)	Amount (%)
A	300	20	KHT	8	71	29
B	300	20	KHT	14	71	29

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TABLE 7

Batch	Amount released Diltiazem (%) after x h (pH 6.8)					Range at 40 % released Diltiazem	
	2h	4h	8h	12h	24h	(%)	n
A	11.4	31.6	62.1	82.4	96.9	5.4	6
B	1.8	14.3	36.8	54.1	85.8	4.4	6

#### Example 2

The following example discloses the stability of the coating according to the present invention.

Cores of Diltiazem, 300 mg, were prepared as previously described and divided into 2 groups. The cores of group 1 were coated with the polymer Eudragit® and the cores of group 2 were coated with the polymer Kollicoat®. Both coatings were prepared with 71% by weight of KHT according to the present invention. The tablets were stability tested for 6 months and the results are shown in the following table 8.

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Table 8

X hours	Eudragit, Amount (%) of released Diltiazem after x hours				
	Initial amount	3 months*	3 months**	6 months*	6 months**
2	7.3	9.4	8.0	8.3	8.5
4	25.5	28.6	27.2	27.4	27.9
8	53.3	58.8	58.1	57.7	59.4
12	74.1	79.3	79.6	78.8	81.2
24	97.4	95.6	96.0	96.4	96.2

X hours	Kollicoat, Amount (%) of released Diltiazem after x hours				
	Initial amount	3 months*	3 months**	6 months*	6 months**
2	9.7	9.1	10.2	9.2	10.6
4	27.8	26.7	28.1	26.6	28.9
8	53.2	52.5	55.5	52.3	56.8
12	69.7	69.2	72.0	68.5	72.9
24	89.4	88.7	89.6	87.4	89.8

\*25°C/75%RH

5 \*\*40°C ambient humidity

As can be seen both groups demonstrated excellent stability properties even in such severe conditions as 6 months in 40°C.